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A magnetic bead immunoassay to detect high affinity human IgG reactive to SARS-CoV-2 Spike S1 RBD produced in *Escherichia coli*

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Abstract

Immunological assays to detect SARS-CoV-2 Spike Receptor Binding Domain (RBD) antigen seroconversion in humans are important tools to monitor the levels of protecting antibodies in the population in response to infection and/or immunization. Here we describe a simple, low cost, and high throughput Ni²⁺ magnetic bead immunoassay to detect human IgG reactive to Spike S1 RBD Receptor Binding Domain produced in *Escherichia coli*. A 6xHis-tagged Spike S1 RBD was expressed in *E. coli* and purified by affinity chromatography. The protein was mobilized on the surface of Ni²⁺ magnetic beads and used to investigate the presence of reactive IgG in the serum obtained from pre-pandemic and COVID-19 confirmed cases. The method was validated with a cohort of 290 samples and an area under the receiver operating characteristic curve of 0.94 was obtained. The method was operated with > 82% sensitivity at 98% specificity and was also able to track human IgG raised in response to vaccination with Comirnaty at > 85% sensitivity. The IgG signal obtained with the described method was well-correlated with the signal obtained when pre fusion Spike produced in HEK cell lines was used as antigen. This novel low-cost and high throughput immunoassay may act as an important tool to investigate protecting IgG antibodies against SARS-CoV-2 in the human population.

Keywords COVID-19 · Magnetic immunoassay · SARS-CoV-2 · High throughput · Magnetic beads

Introduction

In December 2019, a novel beta-coronavirus named SARS-CoV-2 was identified and was responsible for the COVID-19 pandemic [1]. At the end of March 2022, 478,000,000 cases of COVID-19 have been reported and the disease has caused more than 6,110,000 deaths worldwide https://coron

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avirus.jhu.edu/map.html (accessed 30/03/2022). The cycle of SARS-CoV-2 infection stars with the interaction between the Receptor-Binding-Domain (RBD) of the SARS-CoV-2 Spike protein and the human receptor ACE2 [2]. Several studies indicate that human antibodies reactive to SARS-CoV-2 Spike, especially those elicited against the Spike RBD, can neutralize virion particles by blocking the interaction between Spike with the human receptor ACE2 [3, 4]. Hence, a method enabling the identification and quantification of human antibodies reactive to SARS-CoV-2 Spike and Spike RBD can act as an important toll to monitor the level of protecting antibodies to SARS-CoV-2 within the human population.

Since the beginning of the COVID-19 pandemic, several immunological assays were developed and employed to detect human antibodies against SARS-CoV-2 Spike [5–8]. These immunoassays typically use recombinantly expressed and highly purified Spike or Spike RBD to investigate antibodies in human samples. The production of recombinant Spike antigen is usually the costliest factor of an immunoassay. The price of Spike RBD in the market can range between US\$ 2000 and 5000 per milligram https://www. abbexa.com/sars-cov-2-spike-protein-rbd-l452r-mutation (accessed 10/12/2021).

The high cost of production relies on the fact that Spike RBD is obtained using eukaryotic protein expression platforms. Even though cheaper eukaryotic expression systems have been developed including the use of yeast *Pichia pastoris* [9]. The price of production is still high in comparison to proteins produced in prokaryote expression platforms such as *Escherichia coli* [10].

The fact that the SARS-CoV-2 Spike protein is highly glycosylated and contains several disulfide bridges makes this antigen difficult to obtain in *E coli*. The lack of glycosylation systems and the reducing environment typically found in the bacterium cytoplasm results in formation of insoluble inclusion bodies upon expression of Spike in *E. coli* [11]. Some researchers have shown that Spike RBD can be obtained in soluble form from *E. coli* after a denaturation/ refolding procedure and/or by using genetically modified strains with reducing cytoplasm [12–16]. In any case, in all studies where Spike RBD has been obtained from *E. coli*, the antigen seems to have limited antigenicity and low yield [12]. This may explain why there is no report of an accurate immunoassay, validated with a large cohort of samples, which uses Spike RBD produced in *E. coli*.

We have described previously an ultrafast, simple, and inexpensive Ni²⁺ magnetic bead immunoassay which allows detection of human IgG reactive to SARS-CoV-2 nucleocapsid protein using a minimal amount of sample and delivering the results in less than 7 min [17, 18]. The principle of the assay relies on quick and direct mobilization of 6xHistagged version antigens to the surface of Ni²⁺ magnetic beads. We demonstrated that this assay can be used to detect human antibodies reactive to SARS-CoV-2 full length prefusion Spike and to Spike RBD which were recombinantly produced in eukaryotic expression systems.

Here we demonstrate that our previously described assay can also be used to identify human IgG reactive to a fragment of SARS-CoV-2 Spike containing the RBD which was recombinantly produced in *E. coli*.

Materials and methods

Expression and purification of recombinant receptor-binding domain of SARS-CoV-2 spike protein

A codon optimized synthetic gene was produced and cloned into the pET28a vector by General Biosystems. The plasmid construction was named pLHSarsCoV2-S and allowed the expression of a N-terminal 6xHis-tagged fusion of a fragment of SARS-CoV-2 Spike S1 containing part of the N-terminal domain and the full RBD (Uniprot MN908947, M153 to T589). The plasmid construction was transformed into E. coli BL21 (\lambda DE3) and the cells were grown in 100 ml LB medium containing kanamycin (50 µg.ml⁻¹) at 120 rpm at 37 °C to an OD_{600nm} of 0.3. The incubator temperature was changed to 16 °C; after 30 min, IPTG was added to a final concentration 0.3 mM. The culture was kept at 120 rpm at 16 °C overnight. Cells were collected by centrifugation at $3800 \times g$ for 5 min. The cell pellet was resuspended in 10 ml of buffer 1 (Tris-HCl pH 8 50 mM, KCl 100 mM, Urea 8 M). Cells were disrupted by sonication on an ice bath with 8 min cycle, 15 s pulse and 15 s rest, and amplitude 35%. The soluble fraction was recovered after centrifugation at 11.000 rpm for 10 min at 4 °C and loaded into a 5-ml Histrap chelating Ni²⁺ column (Cytiva) which has been previously equilibrated with buffer 1. The column was washed with 20 ml of buffer 1 and bound proteins were eluted with 5 ml of buffer 1 with increasing imidazole 50 mM, 100 mM, 300 mM, and 500 mM. Fractions of 1 ml were collected and analyzed by SDS-PAGE. The fractions containing the protein of interested were polled and the protein was stored in aliquots at -20 °C.

Human samples

Human samples used for the validation of the methodology were collected at Hospital Erasto Gaertner in Curitiba and Federal University of Paraná in Matinhos. Samples for serological analysis comprised both serum and plasma-EDTA. COVID-19 positive cases were confirmed by the detection of SARS-CoV-2 RNA via real-time RT-qPCR from nasopharyngeal sample swabs. The time point of sampling of serum ranged from 1 to 100 days after PCR detection. Among the 86 COVID–positive cases, there were 7 convalescents being 1 asymptomatic and 6 mild non-hospitalized cases. All remaining samples were collected within the first 14 days of the hospitalization period and included 39 severe and 40 critical (intensive care unit). The cohort of 204 negative controls consisted of pre-pandemic samples collected in 2018.

Human samples used to determine if the developed method could be used to track IgG raised in response to vaccination were collected at Federal University of Paraná in Matinhos. Healthy unvaccinated individuals self-declaring no previous SARS-CoV-2 infections were used as controls. Samples from 120 subjects were collected 10 to 30 days after the subjects received the second dose of Comirnaty vaccine (Pfizer-BioNTech—BNT162b2).

The Institutional Ethics Review Board CEP/HEG (n# 31,592,620.4.1001.0098 and n# 54,095,221.0.0000.0098), CEP/UFPR (n# 43,948,621.7.0000.0102 and n# 35,872,520.8.0000.0102) approved this study. Informed consent was obtained from all participants in this study.

All methods were performed in accordance with the relevant guidelines and regulations.

Magnetic bead-based immunoassay

The magnetic bead–based immunoassay was developed using Ni²⁺ magnetic beads as described previously with few modifications [18]. One milliliter of Ni²⁺ magnetic particles MagneHis (Promega cat V8550) was transferred to a 50-ml Falcon tube and washed twice with 1 ml of TBST 1X. The resin was resuspended in 25 ml of TBST 1X and 4 mg of purified N-terminal 6xHis tagged Spike-RBD protein was added. After mixing by inversion, TBST 1X was added to a final volume of 50 ml. The mixture was incubated for 10 min at room temperature with mixing by inversion every 2 min. Beads were washed with 25 ml of TBST 1X and finally resuspended in 5 ml of TBST 1X and stored at 4 °C for up to 2 months.

Assays were performed in 96-well flat-bottom polystyrene microplates (OLEN). An aliquot of 0.8 ml of antigen-loaded beads was resuspended in 10 ml of TBST 1X containing skimmed milk 1% (w/v). After thoroughly mixing, 0.1 ml of the beads was added to each well of the first 96-well plate. The second plate was prepared by adding 0.2 ml of TBST 1X containing skimmed milk 1% (w/ v) and 4 μ l of samples or controls to each well. The wells of plates 3 and 4 contained 0.2 ml of TBST 1X and urea 1 mol/l. Plate 5 contained 0.15 ml of goat anti-human IgG-HPR (Thermo Scientific) at 1/1500 dilution in TBST 1X. The wells of plates 6 and 7 received 0.2 ml of TBST 1X and plate 8 received 0.15 ml of HPR chromogenic substrate TMB (Thermo Scientific).

When all plates were set, reactions started by transferring the beads from plate 1 to 8 and the applying the following incubation times: plates 2 and 5 (2 min); plates 3, 4, 6, and 7 (30 s); and plate 8 (8 min). Beads were gently mixed during incubation. Bead transfer and homogenization were achieved using homemade manually operating magnetic transfer and homogenization device described previously. After completion of the reaction on plate 8, beads were removed; the OD_{650nm} was measured using a Tecan M Nano microplate reader (TECAN) with a bandwidth of 9 nm and 25 flashes.

Data analysis

One COVID-19–positive serum was used as reference throughout the study. Raw data were normalized as percent of this reference before applying Receiver Operating Analysis (ROC) using GraphPad Prism 7.0. Statistical analysis was performed using the t test on GraphPad Prism 7.0.

Results and discussion

We have described previously a nickel magnetic bead immunoassay which was successfully applied to track SARS-CoV-2 seroconversion in humans using either prokaryotic-produced nucleocapsid or eukaryotic-produced full-length Spike or Spike RBD as antigens [18]. The assay is based on the use of commercially available Ni²⁺ magnetic particles which can be directly coated with purified 6xHis-tagged SARS-CoV-2 antigens. The method is amenable to high throughput and can process 96 samples delivering ultrafast results. Despite the simplicity and low cost of the assay, one limiting factor is the price of the Spike and Spike RBD antigens which can be found from 2000 to 5000 US\$/mg on the market.

Previous studies indicated that fragments of the SARS-CoV-2 Spike can be expressed at high levels using *E. coli* as host [13]. However, these constructions are typically produced as insoluble inclusion bodies. Even though soluble protein can be obtained after denaturation/refolding procedures, the antigenicity of these constructions seems to be limited [13, 15]. To the best of our knowledge, there is no commercially available immunoassay based on the use of Spike antigen produced in *E. coli*.

We obtained a synthetic gene which was able to express a fragment of the Spike S1 protein containing part of the N-terminal domain and the full length RBD from the T7 promoter using *E. coli* as expression vector. As expected, based on previous studies, this Spike construction was found as insoluble inclusion bodies after expression [13]. All attempts to reduce protein aggregation which included protein induction at 16 °C, use of detergents during cell disruption, and co-expression with the cysteine reducing system CysDiCo were unsuccessful in solubilizing the Spike antigen (data not shown) [12].

To purify the Spike construction, the *E. coli* cell pellet obtained after protein induction was directly resuspended in buffer containing urea 8 mol/l. Cells were disrupted by sonication and the 6xHis-tagged Spike S1 RBD was purified using Ni²⁺ affinity chromatography using imidazole as eluent; all steps were performed in the presence of urea 8 mol/l. The Spike S1 RBD could be purified 90% homogeneity (Fig. 1) and the protein yield was 120 mg/l of cell culture which is way higher than typically obtained in eukaryotic systems. The estimated cost of consumables for antigen production was US\$ 9 US\$/mg which is 15 × below the price for production of pre fusion Spike in HEK cells [7].

The Spike S1 RBD antigen obtained after affinity chromatography was mobilized to the surface of Ni²⁺ magnetic beads (Fig. 2A). The Spike protein preparation containing urea was incubated with the nickel beads and diluted in TBST buffer in such way that the bead coating step



Fig. 1 Purification of *E. coli* induced Spike S1 RBD. SDS-PAGE analysis of the fractions eluted from the Hitrap chelating column. Lane 1, whole cell extract; lane 2, insoluble fraction; lane 3, soluble fraction; lane 4, flow through; lane 5, wash buffer 1. Other lanes,

fractions collected of the imidazole gradient from 50, 100, 300, to 500 mM. The Spike S1 RBD is indicated by an arrow and eluted between 100- and 500-mM imidazole



Fig. 2 Diagram of the Ni²⁺ magnetic bead immunoassay. **a** Diagram of the resin coating/antigen refolding step. The purified 6xHis tag Spike RBD protein in urea buffer is incubated with commercial Ni²⁺ magnetic particles for 10 min, followed by a wash step in TBST without urea. The beads are ready to use or can be store at 4 °C. **b** Photograph of the 96-pin magnetic extractor device used for 96-well plate

magnetic bead transfer. **c** Diagram of the magnetic immunoassay 8 step process. Bead transfer from plate to plate is performed using the magnetic extractor device followed by manual homogenization for the indicated time (details in reference 8). The final plate contains HPR chromogenic substrate TMB and 8 min incubation is required prior to optical density reading

also acted as Spike refolding step. The development of the immunoassay was based on our previous described method [12]. The investigated serum was incubated with the beads for 2 min, followed by 2×30 s washing steps, 2 min incubation with anti-human IgG HPR conjugate, 2×30 s washing, and final 8 min incubation in chromogenic HPR substrate (TMB) before the measurement of OD_{650nm} using a microplate reader. The complete procedure takes about 15 min (Fig. 2).

A cohort of 28 pre-pandemic and 14 gRT-PCR COVID-19 confirmed serum samples were initially evaluated to determine the best assay conditions. This initial screening revealed that the negative cohort exhibited high background (mean $OD_{650nm} = 0.13$) and they were not clearly distinguished from the COVID-19-positive serum samples (Fig. 3A). Reports on the literature indicate that washing buffers containing urea can be used to reduce the background of negative serum in classic ELISA assays [19, 20]. In fact, use of urea in ELISA washing buffers is a wellestablished method to detect high affinity antibodies. Only antibodies exhibiting high affinity will remain bound to the antigen in the presence of the chaotropic agent. Previous studies indicate that the addition of urea into ELISA wash buffers can increase the specificity of the assay enabling the distinction between closely related diseases such as Zika and dengue [19, 20].

We evaluated if addition of urea to the wash buffers could reduce the background signal of the negative cohort. We noted that the addition of urea 1 mol/l to the wash buffer significantly reduced the background of the negative serum cohort (mean $OD_{650nm} = 0.09$, p = 0.0024) without reducing the signal obtained from the positive serum cohort (Fig. 3A). Hence, urea 1 mol/l was added to the buffers in the two consecutive 30s wash steps after bead incubation with the investigated serum.

After setting the assay conditions, the method was further validated using a larger cohort. The presence of IgG reactive to SARS-CoV-2 Spike S1 RBD antigen was analyzed in sera from 208 pre-pandemic samples and 86 RT-qPCR COVID-19 confirmed cases. The pre-pandemic control sera produced only background signal which was clearly distinguished from the RT-qPCR-confirmed COVID-19 cases (Fig. 3B). Receiver operating characteristic (ROC) analysis revealed an area under curve (AUC) of 0.94 (Fig. 3C). A sensitivity of 82% (73 to 89% at 95% *CI*) could be achieved at a cost of 98% (94 to 99% at 95% *CI*) specificity. These numbers indicate that the method operates with good accuracy.

The biological relevance of the developed assay was further confirmed by the fact the levels of IgG reactive to SARS-CoV-2 Spike S1 RBD antigen produced in *E. coli* was well-correlated with the levels of IgG reactive to prefusion Spike produced in HEK cell lines (Pearson's R = 0.82, Fig. 3D). It is worth mentioning that 4% of the RT-qPCR



Fig. 3 Development of the assay to detect human IgG reactive to S1 RBD expressed in *E. coli*. A Comparison of raw OD_{650nm} obtained with regular TBST buffer or TBST containing urea 1 mol/l. Prepandemic samples are shown in green, and RT-qPCR COVID-19 confirmed cases in red. B Validation of the assay was performed analyzing IgG levels to S1 RBD in pre-pandemic (green) and RT-qPCR COVID-19 confirmed case sera. The assay was also able to detect

IgG in sera obtained from Comirnaty vaccinated individuals (black), unvaccinated (blue). The assay cutoff at > 98% specificity is indicated by the dashed line. **C** ROC curve analysis of the developed assay. **D** The levels of IgG (raw signal OD₆₀₀) reactive to S1 RBD obtained from *E. coli* were well-correlated with the levels detected using Spike obtained from HEK cells as antigen (Pearson's R=0.82, p < 0.0001)

positive cohort did not produce detectable IgG reactive to full length prefusion Spike produced in HEK cells (data not shown) in agreement with previous data where sensitivity of 96% was obtained using prefusion Spike as antigen [18]. Hence, the somehow low sensitivity (82%) obtained in the current study may be, at least in part, explained by the absence of seroconversion in part of the samples used for assay validation.

We determined if the developed method could be used to detect human antibodies raised after vaccination. Of the fifteen samples collected from unvaccinated subjects who reported to have not developed COVID-19, all samples remained below the assay cutoff value (Fig. 3B). On the other hand, of the 120 samples collected from subjects fully immunized with Comirnaty (and reported to have not developed COVID-19), 85% were positive (Fig. 3B). When the same cohort was analyzed for IgG reactive to full length prefusion Spike produced in HEK cells, all samples were positive for IgG (data not shown). These differences in sensitivity may be explained by the limited number of antigen epitopes in the Spike S1 RBD antigen in comparison to the full-length Spike. Furthermore, the presence of urea in the washing buffers is likely to limit the detection of IgG to those antibodies exhibiting high affinity to Spike S1 RBD.

Conclusion

Here we show that E. coli expression system can be used to produce a N-terminal 6xHis tagged SARS-CoV-2 Spike S1 RBD that can be purified at low cost and high yield. The protein retained its antigenic properties when refolded on the surface of nickel magnetic particles and could be used to detect high affinity IgG present in sera from COVID-19-positive cases and from individuals fully immunized with Comirnaty. The method operated with good accuracy, high throughput, and low cost (less than US\$ 1/per sample). To the best of our knowledge, this is the first report to show the feasibility of using Spike produced in E. coli to develop an accurate immunoassay which has been subject to validation with more than 100 samples. We believe that this novel method may act as an important tool to identify and quantify high affinity IgG in human samples reactive to Spike RBD in large scale populational studies.

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Author contribution L.F.H. conceived and designed the study. L.F.H., M.S.C., A.C.G., N.M.P., F.G.M.R., M.N.A., D.L.Z., and J.M.N. collected the samples. L.F.H., M.S.C., and A.C.G. analyzed the data and wrote the paper.

Declarations

Conflict of interest The authors declare no competing interests.

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